Towards Curvature-Based Prediction of Spiral Breakup in Cardiac Tissue

Abhishek Murthy

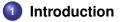
Stony Brook University (SBU)

amurthy@cs.sunysb.edu

Joint Work with Ezio Bartocci, Prof. Radu Grosu and Prof. Scott Smolka

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Wave Breaks and Atrial Fibrillation

Introduction





Introduction



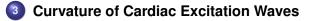
Ourvature of Cardiac Excitation Waves

Case Studies

Introduction



Wave Breaks and Atrial Fibrillation



Case Studies

5 Future Work

- Atrial Fibrillation (AF) the quivering of heart muscles of atrial chambers, is the most common cardiac arrhythmia.
- Prevalent in 2.66 Million Americans, AF responsible for 14,490 deaths in 2010.
- As an independent risk factor for ischemic strokes, responsible for at least 15% to 20% cases.

Cardiac Excitation Waves

- Modelling electrical excitation of cardiac tissue as a reaction-diffusion system - Minimal Model
- Simulating model under Isotropic Diffusion (ID)

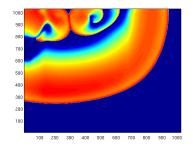


Figure: One time step of simulating cardiac electrical conduction under ID

Wave Breaks and AF

- Spatio-temporal description of the fibrillating cardiac tissue involves wave breaks or phase singularities.
- Curved waves break up near regions of high curvature.

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Predicting wave break-ups will help predict the onset of AF.

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- If V is propagation speed and K, the curvature, then

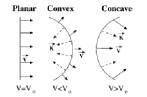
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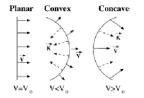
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• Curved waves break near regions of high curvature - wave propagation velocity decreases with increasing convexity. Thus wave breaks up at critical curvature $K_{cr} = V_0/D$

Curvature of Cardiac Excitation Waves

Requirements for estimating and analysing the curvature of excitation waves (for prediction purposes):

- Curvature estimation must be accurate.
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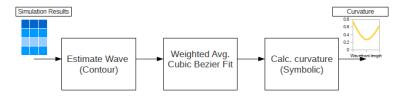


Figure: Curvature Estimation of Cardiac Excitation Waves

 Given a simulation of a grid G of m × n cells, wave W(c, t) can be written as

$$W(c,t) = \{(x,y) | x, y \in \mathbb{R} \ F(x,y) = c \ at \ time \ t\}$$

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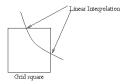


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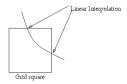


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• Track the same wave across different time steps of the simulation.

Curvature - Cubic Bézier Fits of Waves

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- Fit each of the overlapping strip with cubic Bézier curves of the form:

$$\begin{aligned} X_{j}(t) &= (1-t)^{3} P_{j}^{0} + 3t(1-t)^{2} P_{j}^{1} + 3t^{2}(1-t) P_{j}^{2} + t^{3} P_{j}^{3}. \ t \in [0,1] \ (1) \\ Y_{j}(t) &= (1-t)^{3} Q_{j}^{0} + 3t(1-t)^{2} Q_{j}^{1} + 3t^{2}(1-t) Q_{j}^{2} + t^{3} Q_{j}^{3}. \ t \in [0,1] \ (2) \\ \text{where } j \text{ is the strip index.} \end{aligned}$$

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• In the region of overlap take weighted average of the two curves.

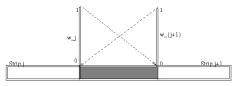


Figure: Weighted average based Bézier curve fitting

Curvature - Symbolic Curvature Estimation

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- If $X_j(t)$ and $Y_j(t)$ denote the fit for a strip, then curvature is calculated as

$$\kappa_j(t) = \frac{|r'_j(t) \times r''_j(t)|}{|r'_j(t)|^3}$$
(3)

where $r_j(t) = [X_j(t), Y_j(t)]$ is the position vector described by the Bézier curve.

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 Continuous closed form of κ_j(t) => continuous curvature estimate along wavefront

(Loading circularCoreCurvatureExample.avi)

- Linear core generated with Minimal Model (1024x1024)
- Spiral Breakup generated with Beeler Reauter Model(1024x1024)

Linear Core

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Linear Core - Curvature Trend

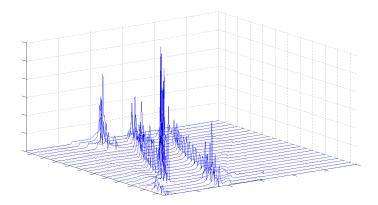
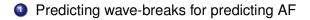


Figure: Curvature trend for linear core till first turn

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- Collect training data by simulating different wave break scenarios.
- Learn patterns of wave break-ups based up morphological features.
- Predict the temporal behaviour using the patterns learnt.



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- Predicting wave-breaks for predicting AF
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- Requirements for curvature estimation
- Weighted average based fitting with cubic Bézier curves
- Symbolic curvature calculation
- Case studies show potential of using curvature to analyse cardiac waves.

References

- "Heart Disease and Stroke Statistics 2011 update: A Report from the American Heart Association", Véronique L. Roger et. al. Circulation Journal of the American Heart Association.
- Measuring Curvature and Velocity Vector Fields for Waves of Cardiac Excitation in 2-D Media", Matthew W. Kay and Richard A. Gray, IEEE Transactions on Biomedical Engineering 2005.
- *Role of Wavefront Curvature in Propagation of Cardiac Impulse, Vladmir G. Fast and André G. Kléber, Cardiovascular Research 1997.
- The Fibrillating Atrial Myocardium. What can the Detection of Wave Breaks Tell Us?", André G. Kléber, Cardiovascular Research 2000.

Consider an edge *e* on the grid *G* whose end points are (x_{g1}, y_{g1}) and (x_{g2}, y_{g2}) and the excitation levels at the two end points are c_1 and c_2 . The wavefront crosses this edge if $c_1 \le c \le c_2$.

Let (x, y) be the point at which the wavefront intersects this edge. x and y can be calculated using linear interpolation as follows:

$$x = x_{g1} + \frac{c - c_1}{c_2 - c_1} (x_{g2} - x_{g1})$$
$$y = y_{g1} + \frac{c - c_1}{c_2 - c_1} (y_{g2} - y_{g1})$$

Running time for n x n grid = $O(n^2)$

Details - Bezier Curve fitting

Bezier curve:

$$X_{j}(t) = (1-t)^{3}P_{j}^{0} + 3t(1-t)^{2}P_{j}^{1} + 3t^{2}(1-t)P_{j}^{2} + t^{3}P_{j}^{3}. t \in [0,1]$$
(4)

$$Y_{j}(t) = (1-t)^{3}Q_{j}^{0} + 3t(1-t)^{2}Q_{j}^{1} + 3t^{2}(1-t)Q_{j}^{2} + t^{3}Q_{j}^{3}. t \in [0,1]$$
(5)
Error functions

$$E_x = \sum_{i=1}^{SL} [x_i - X_j(t_i)]^2$$
(6)
$$E_y = \sum_{i=1}^{SL} [y_i - Y_j(t_i)]^2$$
(7)

which give

$$E_x = \sum_{i=1}^{SL} [x_i - (1 - t_i)^3 P_j^0 + 3t_i(1 - t_i)^2 P_j^1 + 3t_i^2(1 - t_i) P_j^2 + t_i^3 P_j^3]^2$$
$$E_y = \sum_{i=1}^{SL} [y_i - (1 - t_i)^3 Q_j^0 + 3t_i(1 - t_i)^2 Q_j^1 + 3t_i^2(1 - t_i) Q_j^2 + t_i^3 Q_j^3]^2$$

Abhishek Murthy (SBU)

Towards Curvature based Breakup Prediction

Details - Bezier Curve fitting

 P_i^1 and P_i^2 can be obtained at the minimum value of E_x by

$$\frac{\partial E_x}{\partial P_j^1} = 0$$
$$\frac{\partial E_x}{\partial P_j^2} = 0$$

Solving the above two equations we obtain the following expressions for P_i^1 and P_i^2 :

$$P_{j}^{1} = \frac{\alpha_{2}^{j}\beta_{1}^{j} - \alpha_{3}^{j}\beta_{2}^{j}}{\alpha_{1}^{j}\alpha_{2}^{j} - \alpha_{3}^{j^{2}}}$$
(8)
$$P_{j}^{2} = \frac{\alpha_{1}^{j}\beta_{2}^{j} - \alpha_{3}^{j}\beta_{1}^{j}}{\alpha_{1}^{j}\alpha_{2}^{j} - \alpha_{3}^{2}^{j}}$$
(9)

Towards Curvature based Breakup Prediction

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where $\alpha_1, \alpha_2, \alpha_3, \beta_1$ and β_2 for each segment are given by:

$$\alpha_{1} = 9 \sum_{i=1}^{SL} [t_{i}^{2} (1 - t_{i})^{4}]$$

$$\alpha_{2} = 9 \sum_{i=1}^{SL} [t_{i}^{4} (1 - t_{i})^{2}]$$

$$\alpha_{3} = 9 \sum_{i=1}^{SL} [t_{i}^{3} (1 - t_{i})^{3}]$$

$$\beta_{1} = 3 \sum_{i=1}^{SL} [t_{i} (x_{i} - (1 - t_{i})^{3} P_{0} - t_{i}^{3} P_{3})(1 - t_{i})^{2}]$$

$$\beta_{2} = 3 \sum_{i=1}^{SL} [t_{i}^{2} (x_{i} - (1 - t_{i})^{3} P_{0} - t_{i}^{3} P_{3})(1 - t_{i})]$$